

Bioengineering 280A
Principles of Biomedical Imaging

Fall Quarter 2005
MRI Lecture 2

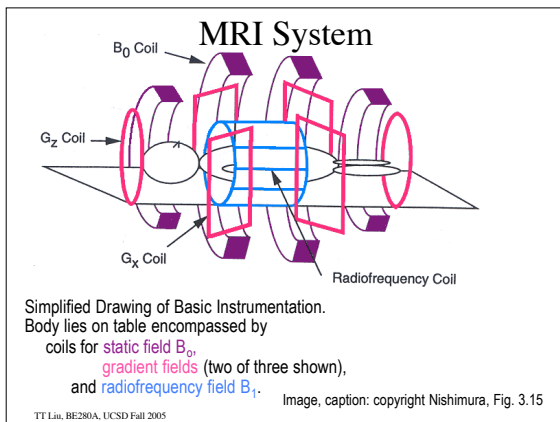
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Gradients

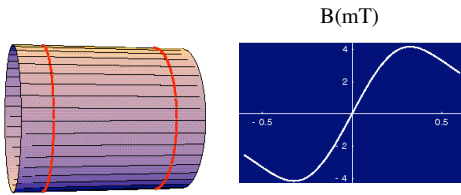
Spins precess at the Larmor frequency, which is proportional to the local magnetic field. In a constant magnetic field $B_z=B_0$, all the spins precess at the same frequency (ignoring chemical shift).

Gradient coils are used to add a spatial variation to B_z such that $B_z(x,y,z) = B_0 + \Delta B_z(x,y,z)$. Thus, spins at different physical locations will precess at different frequencies.

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Z Gradient Coil



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Credit: Buxton 2002

Gradient Fields

$$B_z(x, y, z) = B_0 + \frac{\partial B_z}{\partial x} x + \frac{\partial B_z}{\partial y} y + \frac{\partial B_z}{\partial z} z$$

$$= B_0 + G_x x + G_y y + G_z z$$



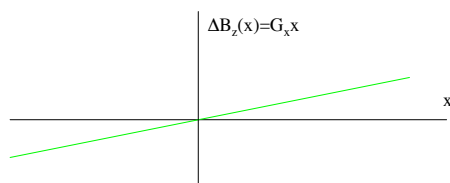
$$G_z = \frac{\partial B_z}{\partial z} > 0$$



$$G_y = \frac{\partial B_z}{\partial y} > 0$$

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Interpretation



Spins Precess at $\gamma B_0 - \gamma G_x x$ (slower)

Spins Precess at γB_0

Spins Precess at $\gamma B_0 + \gamma G_x x$ (faster)

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Gradient Fields

Define

$$\vec{G} \equiv G_x \hat{i} + G_y \hat{j} + G_z \hat{k} \quad \vec{r} \equiv x\hat{i} + y\hat{j} + z\hat{k}$$

So that

$$G_x x + G_y y + G_z z = \vec{G} \cdot \vec{r}$$

Also, let the gradient fields be a function of time. Then the z-directed magnetic field at each point in the volume is given by :

$$B_z(\vec{r}, t) = B_0 + \vec{G}(t) \cdot \vec{r}$$

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Static Gradient Fields

In a uniform magnetic field, the transverse magnetization is given by:

$$M(t) = M(0)e^{-j\omega_0 t} e^{-t/T_2}$$

In the presence of non time-varying gradients we have

$$\begin{aligned} M(\vec{r}) &= M(\vec{r}, 0)e^{-j\gamma B_z(\vec{r})t} e^{-t/T_2(\vec{r})} \\ &= M(\vec{r}, 0)e^{-j\gamma(B_0 + \vec{G} \cdot \vec{r})t} e^{-t/T_2(\vec{r})} \\ &= M(\vec{r}, 0)e^{-j\omega_0 t} e^{-j\gamma \vec{G} \cdot \vec{r} t} e^{-t/T_2(\vec{r})} \end{aligned}$$

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Time-Varying Gradient Fields

In the presence of time-varying gradients the frequency as a function of space and time is:

$$\begin{aligned} \omega(\vec{r}, t) &= \gamma B_z(\vec{r}, t) \\ &= \gamma B_0 + \gamma \vec{G}(t) \cdot \vec{r} \\ &= \omega_0 + \Delta\omega(\vec{r}, t) \end{aligned}$$

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Phase

Phase = angle of the magnetization phasor
 Frequency = rate of change of angle (e.g. radians/sec)
 Phase = time integral of frequency

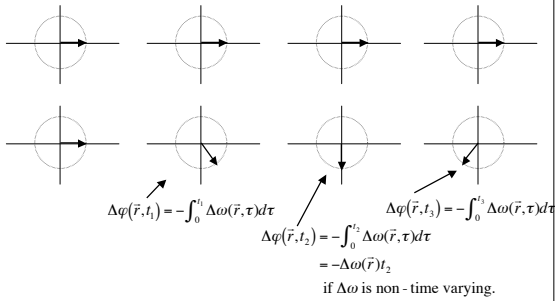
$$\begin{aligned} \varphi(\vec{r}, t) &= -\int_0^t \omega(\vec{r}, \tau) d\tau \\ &= -\omega_0 t + \Delta\varphi(\vec{r}, t) \end{aligned}$$

Where the incremental phase due to the gradients is

$$\begin{aligned} \Delta\varphi(\vec{r}, t) &= -\int_0^t \Delta\omega(\vec{r}, \tau) d\tau \\ &= -\int_0^t \gamma \vec{G}(\vec{r}, \tau) \cdot \vec{r} d\tau \end{aligned}$$

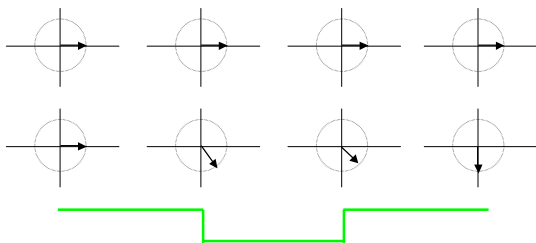
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Phase with constant gradient



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Phase with time-varying gradient



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Time-Varying Gradient Fields

The transverse magnetization is then given by

$$\begin{aligned} M(\vec{r}, t) &= M(\vec{r}, 0)e^{-t/T_2(\vec{r})}e^{i\psi(\vec{r}, t)} \\ &= M(\vec{r}, 0)e^{-t/T_2(\vec{r})}e^{-j\omega_0 t} \exp\left(-j \int_0^t \Delta\omega(\vec{r}, \tau) d\tau\right) \\ &= M(\vec{r}, 0)e^{-t/T_2(\vec{r})}e^{-j\omega_0 t} \exp\left(-j\gamma \int_0^t \vec{G}(\tau) \cdot \vec{r} d\tau\right) \end{aligned}$$

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Signal Equation

Signal from a volume

$$\begin{aligned} s_r(t) &= \int_V M(\vec{r}, t) dV \\ &= \int_x \int_y \int_z M(x, y, z, 0)e^{-t/T_2(\vec{r})}e^{-j\omega_0 t} \exp\left(-j\gamma \int_0^t \vec{G}(\tau) \cdot \vec{r} d\tau\right) dx dy dz \end{aligned}$$

For now, consider signal from a slice along z and drop the T_2 term. Define $m(x, y) = \int_{z_0 - \Delta z/2}^{z_0 + \Delta z/2} M(\vec{r}, t) dz$

To obtain

$$s_r(t) = \int_x \int_y m(x, y) e^{-j\omega_0 t} \exp\left(-j\gamma \int_0^t \vec{G}(\tau) \cdot \vec{r} d\tau\right) dx dy$$

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Signal Equation

Demodulate the signal to obtain

$$\begin{aligned} s(t) &= e^{j\omega_0 t} s_r(t) \\ &= \int_x \int_y m(x, y) \exp\left(-j\gamma \int_0^t \vec{G}(\tau) \cdot \vec{r} d\tau\right) dx dy \\ &= \int_x \int_y m(x, y) \exp\left(-j\gamma \int_0^t [G_x(\tau)x + G_y(\tau)y] d\tau\right) dx dy \\ &= \int_x \int_y m(x, y) \exp\left(-j2\pi(k_x(t)x + k_y(t)y)\right) dx dy \end{aligned}$$

Where

$$k_x(t) = \frac{\gamma}{2\pi} \int_0^t G_x(\tau) d\tau$$

$$k_y(t) = \frac{\gamma}{2\pi} \int_0^t G_y(\tau) d\tau$$

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MR signal is Fourier Transform

$$\begin{aligned}
 s(t) &= \int_x \int_y m(x,y) \exp(-j2\pi(k_x(t)x + k_y(t)y)) dx dy \\
 &= M(k_x(t), k_y(t)) \\
 &= F[m(x,y)]_{k_x(t), k_y(t)}
 \end{aligned}$$

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K-space

At each point in time, the received signal is the Fourier transform of the object

$$s(t) = M(k_x(t), k_y(t)) = F[m(x,y)]_{k_x(t), k_y(t)}$$

evaluated at the spatial frequencies:

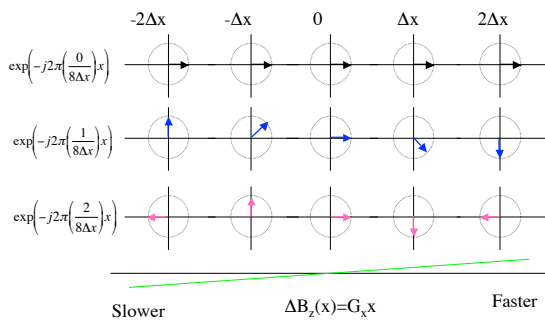
$$k_x(t) = \frac{\gamma}{2\pi} \int_0^t G_x(\tau) d\tau$$

$$k_y(t) = \frac{\gamma}{2\pi} \int_0^t G_y(\tau) d\tau$$

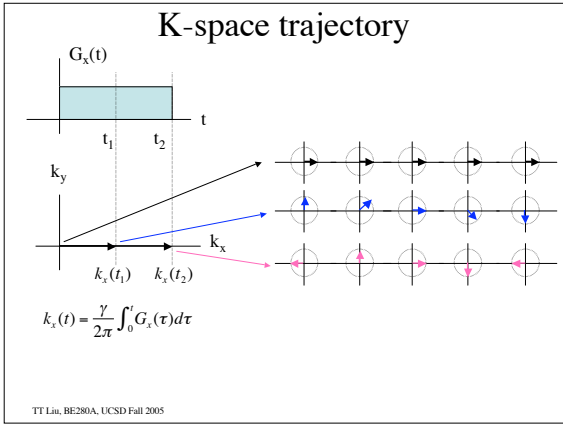
Thus, the gradients control our position in k-space. The design of an MRI pulse sequence requires us to efficiently cover enough of k-space to form our image.

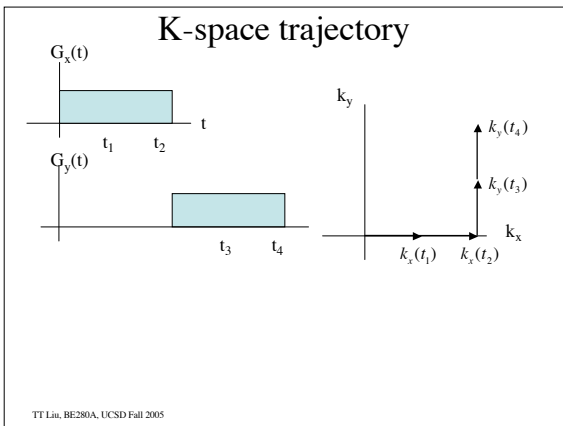
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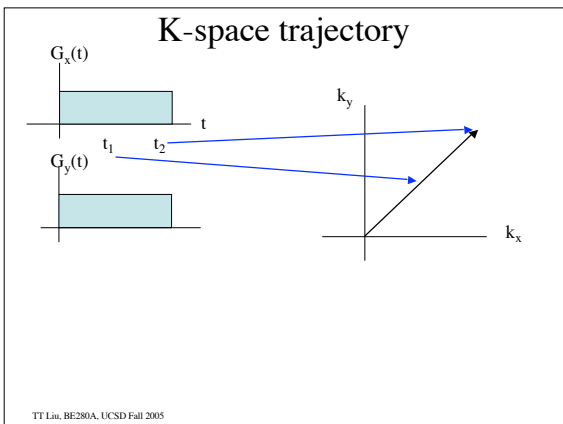
Interpretation

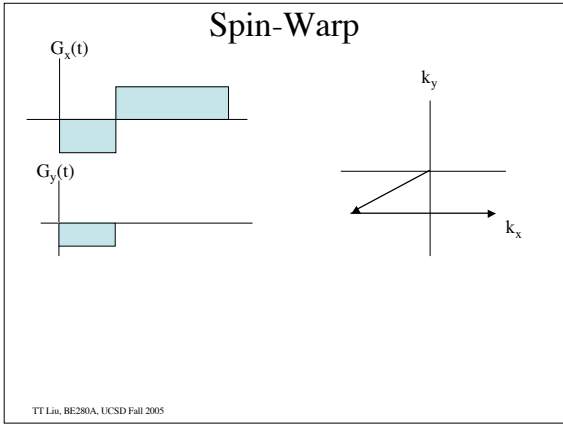


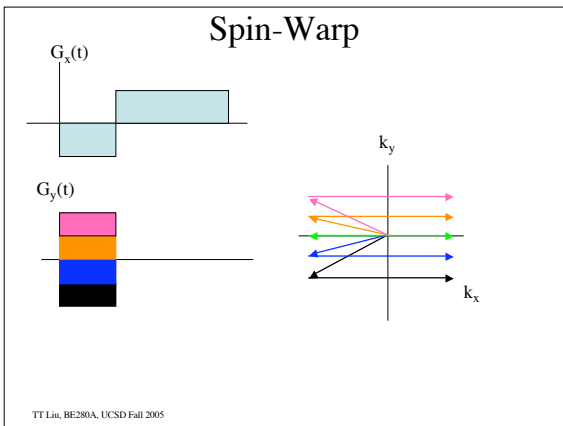
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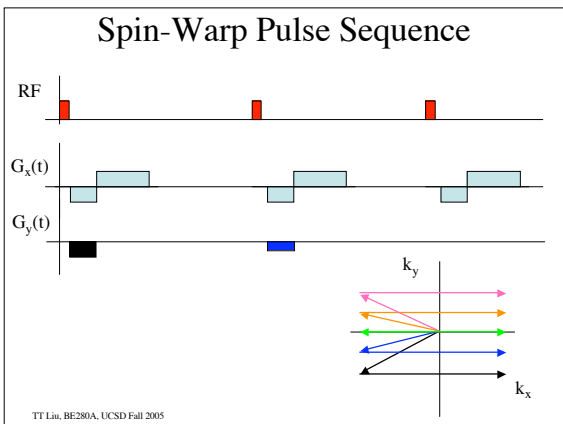












Units

Spatial frequencies (k_x, k_y) have units of 1/distance.
Most commonly, 1/cm

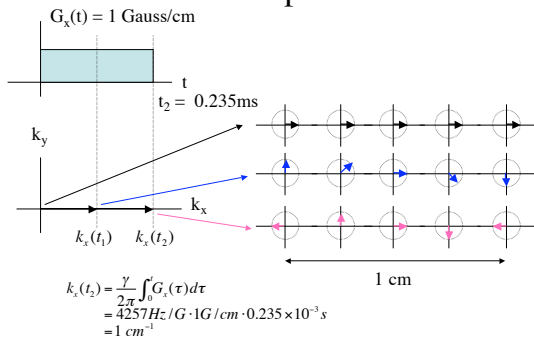
Gradient strengths have units of (magnetic field)/distance. Most commonly G/cm or mT/m

$\gamma/(2\pi)$ has units of Hz/G or Hz/Tesla.

$$\begin{aligned}k_x(t) &= \frac{\gamma}{2\pi} \int_0^t G_x(\tau) d\tau \\ &= [\text{Hz/Gauss}][\text{Gauss/cm}][\text{sec}] \\ &= [1/\text{cm}]\end{aligned}$$

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Example



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